Multiscale Morphological Reconstruction for Hair Removal in Dermoscopy Images

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Abstract

The automatic diagnosis of melanoma is usually affected by the noise that is often included in an image, during the acquisition stage or by superficial factors such as hair. Specifically, hair on the surface of a lesion can cause enough distortion, resulting in an erroneous diagnosis of the region of interest. To solve this issue, several techniques have been presented to detect hair on the surface of a dermoscopy image and substitute a surface approximation for these regions. Nonetheless, the existing methods are prone to false detections or reconstructions that are not uniform, demand high computing resources and modify the textures of important characteristics. Therefore, we proposed a method that detects the hairs by means of a convolution of the image with a kernel belonging to the first derivative of the Gaussian function and replaces the hairs using a multiscale morphological reconstruction. In addition, we integrated a refining stage that contributes to maintaining the quality of the patterns on the lesion. We used 36 dermoscopy images in the evaluation, which included a total of 586 hairs that were automatically detected with the proposed process and validated with their respective manual segmentations. Our results showed sensitivity and specificity performance measurements of 94.14% and 99.89%, respective.

Keywords: dermoscopic images, region of interest, derivative of gaussian, dark lines detection, morphological reconstruction

1. Introduction

Among many types of cancer, skin cancers are the most common form of cancers in human (Bhuiyan, et. al. 2013, pp. 1-6). This cancer is the sixth most common one among American men and women and is the main factor of cancer death in 25-30 years old women. Also, melanoma is the most common type of cancer in 20-44 years old men in Australia and New Zealand (Ramezani, et. al. 2014, pp. 281–290) (Kutlubay, et. al. 2013. pp. 67–125). Because timely detection of this cancer can extend the patient's life considerably (Sadeghi, et. al. 2011, pp. 137–143) (Abbas, 2011, pp. 91–100), specialists have made various contributions to the development of new methods that contribute to the early diagnosis of melanoma, specifically in visual examination procedures. Among these methods are the ABCD Rule (Soltani, et. al. 2015, pp. 412-500), the Menzies method (Menzies. 1996, pp. 1178–1182), and the 7-point checklist (Argenziano, et. al. 1998, pp. 1563–157). However, the diagnostic process is not sufficiently precise. Therefore, optical tools that enlarge the dimensions of the image are frequently used to broadly define the variety of malignant structures within the lesion. Dermoscopy is a magnifying diagnosis technique using polarized light that has proven to be useful in the categorization of melanocytic proliferations (Cymerman, et. al. 2015, pp. e197-e208). Despite efforts to increase the accuracy of melanoma diagnoses, the estimated precision for expert dermatologists is within the range of 75-84%.

In order to increase the performance in melanoma diagnosis, several automatic diagnosis systems have been developed (Li, et. al. 2014). These diagnostic systems have been developed in recent years, due to the contribution they can make to the specialist's decision-making process (Ali, et. al. 2012) (Capdehourat, et. al. 2011, pp. 2187–2196). These methods employ techniques that reduce the subjectivity associated with traditional diagnostic methods and they can emphasize important details that are usually not observable by the human eye. Segmentation is one of the main processing tasks of this type of system. This step is perhaps the most affected by the quantity of noise, frequently observed as a number of bubbles, pores, scale marks or hairs (Abbas, et. al.

2010, pp 1-15). All these types of noise usually make the results inefficient. Within these common factors, hairs are the most harmful since they are located randomly on the surface of the image and can be found in regions associated with the lesion, obstructing crucial characteristics such as its edges. To diminish the impact of this noise, a preprocessing stage is generally developed.

This stage can include: a color transformation to reduce the negative contribution of noise (Kutlubay, et. al. 2013. pp. 67–125) (Xu, et. al. 1999, pp. 65–74) (Rajab, et. al. 2004, pp. 61–68) (Mendonza, et. al.2010, pp. 531–540), the softening of the image by means of spatial filters, specifically by the average filter (Celebi, et. al. 2008, pp. 347–353), the combination of the previous two methods (Sadeghi, et. al. 2011, pp. 137–143) (Celebi, 2009, pp. 148–153) or the implementation of new specialized methods for noise removal (Ramezani, et. al. 2014, pp. 281–290) (Abbas, 2011, pp. 91–100) (Lee, et. al. 1997, pp. 533–543), particularly, methods specific to hair elimination.

Hair removal is an issue of wide interest for automatic melanoma treatment (Somnathe, et. al. 2015, pp. 73-76). In general, the automatic hair removal procedure has three stages. First, a model of the hairs is proposed; subsequently, the hairs are detected and finally, the hairs are removed from the image by substitution. Reports indicate that hair modeling can be performed based on a series of profiles that define the hair (Abbas, 2011, pp. 91-100) by means of convolution, with the kernel corresponding to the partial derivative of the Gaussian function (Jaworek, 2015) or by means of background elimination obtained through morphological operations with special structures, such as rectangular structures rotated at 0° , 45° and 90° (Lee, et. al. 1997, pp. 533–543) (Saugeon, et. al. 2003, pp. 65-78). After detecting the hairs by means of the proposed model, the challenge consists in obtaining a surface that works as an appropriate substitute for the regions where the hairs are found and correct the false detections generated in the previous stage. To solve this problem, the intensities adjacent to the regions the hairs are employed by means of linear interpolation techniques (Lee, et. al. 1997, 533–543). The restoration is made based on partial differential equations (Criminisi, et. al. 2004, pp. 1–13), or a new surface is generated based on the morphological closing operation (Saugeon, et. al. 2003, pp. 65–78). In the literature, there exist several publications about hair removal in dermoscopic image. For instance, in (Abbas, et. al. 2013, e27-e36), a novel hair-restoration algorithm is presented, which has a capability to preserve the skin lesion features such as color and texture and able to segment both dark and light hairs. The algorithm is based on the rough hairs are segmented using a matched filtering with first derivative of Gaussian (MF-FDOG) with thresholding that generate strong responses for both dark and light hairs, refinement of hairs by morphological edge-based techniques.

Although these methods have the ability to detect hair, it is necessary to search for methods that do not detect other regions of interest that affect the texture and modify the discriminating patterns in malignancy recognition. Additionally, it is difficult to assess the exact performance of these methods because the performance analyses is determined in a qualitative way.

Therefore, in this document, we propose a study designed for hair removal as well as effective substitution of the hair by applying an iterative morphological reconstruction approach without altering the characteristics of the lesion. In addition, we propose an assessment method to obtain the traditional performance measurements (sensitivity and specificity) so that the specialist's criteria are integrated successfully and in a timely manner. Thus, the proposed method is evaluated both, qualitatively and quantitatively, under the supervision of a team of two specialists in the detection of dermatological pathologies. This Article is divided as follows:

Section 2 introduces the proposed method. Section 3 offers a discussion of the experimental results, and section 4 presents the conclusions.

2. Material and Methods

Figure 1(a) shows a dermoscopic image presenting a possible melanoma, including natural hairs; furthermore, in this image the magnification of a region exhibiting a hair that vertically oriented unfolds is included. The cross-section of the same area and its respective three-dimensional representation is presented in figure 1(b). As observed in this figure, the image includes the region associated with the depression caused by the presence of the hair that can be presented in multiple orientations.





Since hairs are particularly distinguishable by their lengthened, thin structures and in many cases, dark tones, hair recognition is conducted based on the detection of the most similar geometric structure as dark lines (Abbas, et. al. 2010, pp 1-15) (Li. 2008). For this procedure, the algorithm presented in the diagram of figure 2 is proposed. Each procedure included in this algorithm will be deeply explained below in this document.

Generally, the detection of dark lines is conducted based on the use of the second derivative of the Gaussian function; nevertheless, it is well known that this method produces a non-desirable response to objects with light tonalities. For solving this issue, a method using the convolution of the image with a window associated to the first derivative of the Gaussian function is proposed (Mendonza, et. al.2010, pp. 531–540). This method suggests the hair detection using its cross section.



Figure 2. General diagram of the method proposed for hair removal

In (Saugeon, et. al. 2003, pp. 65–78), the researchers showed that the kernel associated with the derivative of the Gaussian function performs efficiently in the detection of dark lines, generating more exact responses. Because the melanocytic lesions have relevant patterns with light tones (e.g., reticular pattern, blue-white veil and edges), in this work we employ the Derivative of Gaussian (DOG) function presented in equation (1). Let X be the array referring to the kernel's spatial region in the axis x and y. And let Σ be the covariance matrix of X

$$g'(X) = -\frac{x}{\sqrt{2\pi}|x|} e^{-\frac{1}{2}x^T x^{-1} x}$$
(1)

If an ideal case of a depression is considered, as is shown in figure 3(a), the convolution obtained using the DOG function kernel is shown in figure 3(c). Observing this figure, it is concluded that the center of the depression is located in the middle of two extreme points having opposite signs. However, in real cases, According to the cross-section of the image shown in figure 1(a) as a red line (in color image) this cross section behaves as is indicated in Figure 3(b), were several fluctuations are observed due to the noise, pores or changes in lighting. The result of calculating the profile convolution with the DOG kernel to obtain the signal for this real image is shown in 3(d). In this figure, the center of the depression is not necessarily placed at the middle of the two extremes. For solving this issue, a simple solution is proposed, as is explained bellow, using a 2D convolution.



Figure 3. (a) Ideal profile of a hair, (b) Profile the hair in normal conditions, (c) convolution of the ideal hair with the DOG Kernel and (e) Convolution of a normal hair using the DOG Kernel.

Based on the concepts exposed before, the procedure can be extrapolated to two dimensions. Here, the DOG kernel can be rotated to an angle θ , guaranteeing the detection of the multidirectional hairs, having into account that hairs are randomly oriented. It is important to take care in rotated the kernel around its principal axis. Since there exists a lot of orientations, and to rate the kernel around all of them implies a great computational cost, the experimental results suggest that the angles 0°, 45°, 90° and 135° can be chosen to identify the randomly oriented hairs. The kernel rotation is performed using equations (2).

$$x' = x\cos(\theta) + y\sin(\theta)$$

$$y' = y \cos(\theta) - x \sin(\theta)$$
(2)
$$X = [x' \ y']$$

Where x and y are the non-rotated coordinates, while x' and y' are the rotated coordinates. With these equations, the kernel rotated in the proposed angles is generated, as is shown in figure 4. At this point, the convolution guarantees that the kernel g'(x,y) will be applied on all the image surface I(x,y), generating as a result, a filtered image F(x,y), according to equation (3)

$$F_{i}(x,y) = I(x,y) * g_{i}'(x',y')$$
(3)

Finally, the identification of the center of each hair can be determined by means of equation (4).

$$Cn_{i} = \begin{cases} F_{i}(x - d, y) + |F_{i}(x + d, y)|, & if (x - d, y) > 0 \text{ and } F_{i}(x + d, y) < 0 \\ 0, & 0 \text{ therwise} \end{cases}$$
(4)

Each *i*-th array of the preceding expressions corresponds to a specific rotation of the employed kernel. For the integration of all the arrays C_{ni} , the maximum intensity associated with the pixel at the position (x,y) is selected, according to equation (5).

$$R(x,y) = max(Cn_i(x,y))$$
⁽⁵⁾



Figure 4. Bidimensional DOG kernel, rotated in the main angles (a) 0°, (b) 45°, (c) 90° and (d) 135°.

Figure 5(a) shows the original Dermoscopy image. As a result of the combination of the C_{ni} channels determined after processing the original image, a new image containing structures corresponding to the dark lines (hairs) is obtained; however, undesired structures are also included, as shown in Figure 5(b). These undesired regions are

eliminated with the application of a thresholding algorithm (Otsu Method). With this algorithm, a morphological operation was previously applied over the image R(x,y). The morphological operation implicitly balances the histogram for the image R(x,y). This histogram allows to discover a more discriminating threshold in the classification of the tones associated with the background and the hair. A square geometric structure was selected as the morphological structure with a windowing dimension ws = 5. A filter was applied to eliminate insignificant objects after the thresholding (Figure 5(c)), removing objects with areas of sizes lower than 20 pixels. Consequently, a partial binary mask M_{kp} is automatically generated for the hairs presented in the original image (Figure 5(d)). As the area of the morphological structure increases, the thresholding algorithm accepts region with tones similar to the region of interest, but do not belong to it, being more imprecise.



Figure 5. (a) Dermoscopy image including hairs, (b) Image R(x,y) resulting from the detection procedure of dark lines, (c) Detection of the relevant structures using thresholding and (d) M_{kp} mask associated with hair dispersion

2.1 Refining Stage

Because we attempt to remain the relevant texture of the original image (figure 6(a)) and patterns of the region of interest (ROI), this study proposes a refinement stage, in order to eliminate the false screenings of the previous stage. For this reason, a stage that claims few computing resources while conducting this task efficiently is developed. The Otsu method is a popular technique that is known for its efficiency (Otsu, et. al. 1979, pp. 62–66). In this case, this method is employed to obtain a preliminary detection of the lesion (Figure 6(b)), where the entry image belongs to the rectangular area associated with the region of interest (ROI), as shown in Figure 6(a). The ROI surface is essentially obtained with the definition of the sudden changes in intensity within the original image when the scanning is carried out from the top to the bottom and then, from the left to the right. The initial

(b)

segmentation (Figure 6(b)) will be used to limit the hair mask exclusively to regions outside the lesion. The result of this process is the mask M_k , presented in Figure 6(c).



Figure 6. (a) Extraction of the region of interest (ROI), (b) Partial lesion segmentation and (c) Final M_k mask associated with hair dispersal

2.2 Substitution

After obtaining the binary mask M_k , (Figure 6(c)) that defines the areas occupied by the hairs on the surface of the original image I(x,y), morphological operations are used to find an uniform surface approximation S_a , belonging to the image texture, that is suitably substituted by the regions associated with the hair.

Accordingly, let's consider the original image without the regions associated to the hairs, presented in Figure 7(a). Let us suppose that this image is dilated n times. In each iteration, the morphological structure grows linearly; for this reason, the empty spaces (corresponding to the region occupied by the hair) gradually disappear as new intensities (belonging to the skin texture) occupy the region. Considering the previous concept, the surface S_a is built with new intensities that fill the holes after the image is dilated using a circular structure with a growing radius. To guarantee a uniform and exact surface, only the intensities that entered the region for the first time are kept, without taking the intensities found in the previous scale into account. Figure 7(b) illustrates the pixel insertion process.



(a)

Figure 7. (a) Original dermoscopy image without hair-associated regions. (b) Surface substitution growth process.

Please note that each scale is assigned to a specific color and only eight iterations are required to obtain the new surface. In the first iteration, we obtain the pixels located at the edges of the object, which have a blue intensity. As the scale grows, new pixels are accepted in this way until all regions defined in the mask M_k are eliminated; in this case, they are represented by shades of dark red. The final intensity of the discovered pixels is determined

from the dilation in which they were obtained. The final substitution surface will be the sum of the contribution of the n-th dilation, as in equation (6).

$$S_a = S_{a1} + S_{a2} + S_{a3} + \dots + S_{an}$$
(6)

Each image S_{ai} is calculated having into account the pixels that have already occupied some region within the mask. This procedure is carried out for avoiding a previous consideration of them in a new search. As a result, each iteration depends on the previous one. The S_a approximation image was calculated by means of equation (7).

$$S_{\alpha} = \sum_{i=1}^{n} \left([\mathbb{I} \bigoplus M_{k}] \times W_{i} \times \right) \left[\underbrace{\bigcup_{j=1}^{i-1} \mathbb{BW}(S_{\alpha j})}_{\mathbb{I}} \right]^{n}$$
(7)

where $\mathbb{BW}(S_{\alpha,j})$ corresponds to the binary image of all the values different from zero in the image S_{aj} . Operator \bigoplus refers to dilation operation between image \mathbb{I} and W_i that represents the circular kernel structure with increasing radius *i*. The operation \mathbb{I}^e is equivalent to the complement of the binary image \mathbb{I} , and operation $M_{kc} \times \mathbb{I}^e$ corresponds to the point-to-point products of both matrixes. Finally, the expression required to calculate the hair-free image H_L is indicated in equation (8), which essentially eliminates the regions covered by hairs (Figure 7(a)). Later, these regions are replaced with the obtained surface S_a , as in Figure 8(a). The resulting image H_L , devoid of hairs, is shown in Figure 8(b).



Figure 8. (a) Surface rebuilt by means of the proposed substitution process and (b) Image resulting from the proposed hair-removal process.

$$H_L = \underbrace{I.M_k^c}_{A} + \underbrace{S_a}_{B} \tag{8}$$

Where $M_k^{\mathcal{E}}$ represents the complement of the mask M_k . In other words, the regions indicated by the complement of regions tagged as hairs are left intact but only gaps are filled with the new estimated surface S_a . The mask is applied to all channels in the color image and S_a can be found for each channel separately by using the method described above.

2.1 Experimental Frame

A quantitative and qualitative comparative study was developed under the supervision of a team of two specialists in dermatology from the University of Caldas. A database comprising 36 dermoscopic images was acquired under a specific acquisition protocol for being used in this study. Most of these images exhibited a strong presence of hairs on surface, while the remainder only showed metric marks. All the images were captured with a DermLite II Pro dermatoscope connected to a Canon PowerShot A2200 camera. These images were digitalized in RGB-Color format with an initial dimension of 1200x1600. They were later reduced to a third of that size for processing without any loss of information. The implementation of the proposed methods

was conducted in Matlab© R2008a, and evaluated using a computer with a 2.4 GHz Intel Core i5 processor with 3 GB RAM of memory.

3. Results

To evaluate the performance, the hair mask was extracted manually from both, the original and the processed images. Since there exists a great presence of hairs in the image, the manual detection of these hairs is a laborious task. To solve this issue, hairs were modeled using few points selected by a specialist, as shown in Figure 9(a). The points are used to generate a curve by means of splines and then to generate a binary image where the lines represent the original hairs mask obtained with the expert selection, as in Figure 9(b). In this way, the task of manual detection of the hairs is drastically reduced. From the database, 36 images were selected and into them, 586 dark lines were detected manually. These lines are formed by hairs and metric marks. On average, the dispersion of hairs and metric marks comprised 3.2% of the original surface per image. These hairs and marks are then defined as variable characteristics specifically in terms of coloring, width, length and tortuosity.



Figure 9 (a). Manual hairs identification in the original image using the points selection and splines fitting, (b) Binary image obtained from the manual identification procedure applied to the original image, (c) hairs identification applied to the processed image and (d) binary image obtained after the manual hairs detection for the processed image

The result of the hair selection procedure is the generation of two binary images: one that represents the mask M_{ko} of the hairs extracted from the unprocessed image (Figure 9(b)) and one that corresponds to the mask M_{ka} of the hairs that were not detected with the proposed method (Figure 9(d)), indicating that the other hairs were identified and appropriately substituted.

However, because the aim of this work is to determine the performance of the detection method, the image where the hairs were successfully detected is obtained. The calculation is generated by means of the subtraction of both masks, as shown in equation (9).

$$M_{kd} = M_{kg} - M_{kg} \tag{9}$$

Finally, the precision of the methods can be expressed quantitatively in terms of sensitivity and specificity. The formulas employed for obtaining parameters used for determining sensitivity and specificity are shown in table 1 and their values are presented in table 2.

Table 1. Variables used to calculate performance.

Definition	Formula
True Positive	$T_p = \sum_{k} \sum_{j} (M_{k0} \times M_{kd})$
True Negative	$T_n = \sum_{i} \sum_{j} [(I - M_{k0}) \times (I - M_{kd})]$
False Positive	$F_p = \sum_{k} \sum_{j} [(I - M_{k0}) \times (M_{kd})]$
False Negative	$F_n = \sum_{k} \sum_{j} [(M_{k0}) \times (I - M_{kd})]$
Sensitivity	$S_n = T_p \left(T_p + F_n \right)^{-1}$
Specificity	$S_p = T_n \left(T_n + F_p \right)^{-1}$

In addition to the proposed method, the development assessment included the popularly employed technique for hair removal, DullRazor. The performance values of both methods of hair detection are shown in Table 2. The results indicate the superiority of the proposed method to efficiently detect hair.

Table 3. General p	performance o	of the methods	used for	hair removal
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Method	Hair	Mask	Performance	
	Detection	Substitution	Sens. %	Espec. %
DullRazor	Closing Morphology Operation	Bilinear Interpolation.	88.65	99.81
Proposed	DOG Convolution, Thresholding	Multiscale Morphology Reconstruction	94.14	99.89

In accordance with the qualitative analysis conducted by the team of specialists, the proposed method does not affect the quality of the image, nor does it insert noise or damage the regions of study of the lesion. In fact, the DullRazor method does not adequately rebuild the regions covered by the hairs, adding discontinuities, diffusing regions and mixing colors in the final image. We simultaneously studied the algorithm exemplar-based image inpainting (Abbas, et. al. 2010, pp 1-15) (Criminisi, et. al. 2004, pp. 1–13) given for the substitution of the hair-covered regions. However, the exaggerated computational cost required to obtain the surface covered by a single hair was obvious, and although the approximation is also built based on the surface surrounding the hairs, this method did not generate an adequate representation.

4. Conclusions

An important discriminating characteristic for the identification of melanoma is the lesion edges, which generally exhibit a low contrast and the distinctive noise inherent in pigmented skin lesions. Specifically, the hair

and the nonhomogeneous illumination are the most problematic patterns, making the automatic detection of the lesion a complex and inexact task.

This study employed the convolution of the image for being used in hair detection and removal, with a window corresponding to the first derivative of the Gaussian function rotated in the main angles. In addition, we proposed including a refining stage, which main task is to filter out the false detections located on the lesion surface. Finally, and as the main contribution of this study, we proposed a stage for the replacing the hairs based on the multiscale morphological reconstruction.

The result of the refining stage was the ability to preserve the texture and the different characteristics located on the region of interest. Regarding the presence of hairs placed outside the lesion, we found an adequate surface that uniformly corresponds to the areas associated with the skin. The experimental results suggest that the general proposed technique adequately removes the hairs located on the surface of the dermoscopy image, generating hair detection performances with sensitivity and specificity values equivalent to 94.14% and 99.89%, respectively.

In general, the method presented in this study detects and efficiently replaces the hairs present in the image, surpassing the general performance of the popularly employed technique

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References

- Abbas, Q., Celebi, M. E, García, I. F, & Rashid. M. (2011). Lesion border detection in dermoscopy images using dynamic programming. *Skin Res. Technol.*, *17*, 91–100. https://doi.org10.1111/j.1600-0846.2010.00472.x
- Abbas, Q., Fondón Garcia, I., Celebi, M. E., & Ahmad, W. (2013). A Feature Preserving Hair Removal Algorithm for Dermoscopy Image. *Skin Research and Technology*, *19*, 2013, e27-e36. https://doi.org/10.1111/j.1600-0846.2011.00603.x
- Abbas, Q., Fondon, I., & Rashid, M. (2010). Unsupervised skin lesions border detection via two-dimensional image analysis. *Comput. Meth. Prog. Bio., 104*, 2010, 1-15. https://doi.org/10.1016/j.cmpb.2010.06.016
- Ali, A.-R. A., Deserno, & Thomas M. (2012). A Systematic Review of Automated Melanoma Detection in Dermatoscopic Images and its Ground Truth Data. Proc. of SPIE, 8318, 2012, 83181I-1. https://doi.org/10.1117/12.912389
- Argenziano, G., Fabbrocini, G., Carli, P., Giorgi, V. D., Sammarco, E., & Delfino, M. (1998). Epiluminescence microscopy for the diagnosis of doubtful melanocytic skin lesions, comparison of the abcd rule of dermatoscopy and a new 7-point checklist based on pattern analysi. Archives of Dermatological Research, 134, 1563–157. https://doi.org/10.1001 / archderm.134.12.1563
- Bhuiyan, Md. A. H., Azad, I., & Uddin, Md. K. (2013). Image Processing for Skin Cancer Features Extraction. *Inter. J. Sci. Eng. Res.*, 4, 1-6. https://doi.org/10.1016/j.procs.2015.04.209.
- Capdehourat, G., Corez, A., Bazzano, A., Alonso, R., & Musé, P. (2011). Toward a combined tool to assist dermatologists in melanoma detection from dermoscopic images of pigmented skin lesions. *Pattern Recognition Letters*, *32*, 2187–2196. https://doi.org/10.1016/j.patrec.2011.06.015
- Celebi, M., Iyatomi, G. S. H, & Stoecker, W. V. (2009). Lesion border detection in dermoscopy images. *Computerized Medical Imaging and Graphics, 33,* 148–153. https://doi.org/10.1016/j.compmedimag.2008.11.002
- Celebi, M. E, Kingravi, H. A., Iyatomi, H., Aslandogan, Y. A, Stoecker, W. V., Moss, R. H, Malters, J. M., Grichnik, J. M., Marghoob, A. A., Rabinovitz, H. S., & Menzies, S. W. (2008). Border detection in dermoscopy images using statistical region merging. *Skin Research Technology*, 14, 347–353. https://doi.org/10.1111/j.1600-0846.2008.00301.x
- Criminisi, A., Perez, P., & Toyama, K. (2004). Region filling and object removal by exemplar-based image inpainting. *IEEE Transactions on Image Process*, 13, 1–13. https://doi.org10.1109/TIP.2004.833105
- Cymerman, R. M., Penn, L., Meehan, S., & Polsky, D. (2015). Polarized light dermoscopy to aid in the diagnosis of new pink lesions in an amelanotic melanoma survivor. *J. Am. Acad. Dermatol.*, 73, 2015, e197-e208. https://doi.org/10.1016/j.jaad.2015.08.048

- Jaworek-Korjakowska, J. (2015). Novel Method for Border Irregularity Assessment in Dermoscopic Color Images. Computational and Mathematical Methods in Medicine, 2015, Article ID 496202. http://dx.doi.org/10.1155/2015/496202
- Kutlubay, Z., Engin, B., Serdaroğlu, S., & Tüzün, Y. (2013). Current management of malignant melanoma: State of the art. in Highlights in Skin Cancer, Estanbul, Turquía, 67–125. https://doi.org10.5772 / 55304
- Lee, T., Ng, V., Gallagher, R., Coldman, A., & McLean, D. (1997). DullRazor: A software approach to hair removal from images. *Comput. Biol. and Med.*, 27, 533–543. https://doi.org/10.1016/S0010-4825(97)00020-6
- Li, L., Zhang, Q., Ding, Y., Jiang, H., Thiers, B. H., & Wang, J. Z. (2014). Automatic diagnosis of melanoma using machine learning methods on a spectroscopic system. *BMC Med Imaging.*, 14, 36. https://doi.org/10.1186/1471-2342-14-36
- Li, Q., Zhang, L., You, J., Zhang, D., & Bhattacharya, P. (2008). Dark line detection with line width extraction. In IEEE International Conference on Image Processing, Hong Kong, China. https://doi.org/10.1109/ICIP.2008.4711831
- Mendonza, T., Marcial, A., Vieira, A., Nascimento, J., Silveira, M., Marques, J., & Rozeira. J. (2010). Comparison of segmentation methods for automatic diagnosis of dermoscopy images. *Image and Signal Processing: 4th International Conference*, 1, 2010, 531–540. https://doi.org/10.1109/IEMBS.2007.4353865
- Menzies, S., Ingvar, C., Crotty, K., & McCarthy, W. (1996). Frequency and morphologic characteristics of invasive melanoma lacking specific surface microscopic features. Archives of Dermatological Research, 13, 1178–1182. https://doi.org/archderm.1996.03890340038007
- Otsu, N. (1979). A threshold selection method from gray-level histograms. *IEEE Transactions on Systems, Man. and Cybernetics*, 9, 1979, 62–66. https://doi.org/10.1109/TSMC.1979.4310076.
- Rajab, M., Woolfson, M., & Morgan, S. P. (2004). Application of region-based segmentation and neural network edge detection to skin lesions. *Computerized Medical Imaging and Graphics*, 28, 61–68. https://doi.org/10.1016/S0895-6111(03)00054-5.
- Ramezani, M., Karimian, A., & Moallem, P. (2014). Automatic Detection of Malignant Melanoma using Macroscopic Images. J. Med. Signals Sens., 4, 281–290. https://doi.org/10.1016/0895-6111(92)90073-I.
- Sadeghi, M., Razmara, M., Lee, T. K, & Atkins. M. S. (2011). A novel method for detection of pigment network in dermoscopic images using graphs. *Computerized Medical Imaging and Graphics*, 35, 137–143. https://doi.org/10.1016/j.compmedimag.2010.07.002
- Saugeon, P. S, Guillod, J., & Thiran, J. P (2003). Towards a computer-aided diagnosis system for pigmented skin lesions. *Computerized Medical Imaging and Graphics.*, 27, 65–78. https://doi.org/10.1016/S0895-6111(02)00048-4
- Soltani-Arabshahi, R., Sweeney, C., Jones, B., Florell, S. R., Hu, N., & Grossman, D. (2015). Predictive value of biopsy specimens suspicious for melanoma: support for 6-mm criterion in the ABCD rule. J Am Acad Dermatol., 72, 412-500. https://doi.org/10.1016/j.jaad.2014.11.030
- Somnathe, P. A., & Gumaste, P. P. (2015). A Review of Existing Hair Removal Methods in Dermoscopic Images. *IOSR Journal of Electronics and Communication Engineering*, 2015, 73-76. https://doi.org10.1111/srt.12015.
- Xu, L., Jackowski, M., Goshtasbya, A., Roseman, D., Bines, S., Yu, C., Dhawan, A., & Huntley, A. (1999). Segmentation of skin cancer images. *Image and Vision Computing.*, 17, 65–74. https://doi.org/10.1016/S0262-8856(98)00091-2.

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